

# Numerical analysis of effective pressure on microfluidic aspiration of a single cell before constriction

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## Introduction

Several techniques exist to evaluate the cell behavior under mechanical stresses, mainly analyzing its stiffness and deformability, properties related to the internal structure and biomarkers. A commonly used procedure to test deformability of cells is to **study their flow through constrictions**. High throughput devices, like Microfluidic devices, once manufactured and put into operation, do not require long training and the equipment is relatively cheap compared to others. **However several authors have reported great variability in the results of cell deformability and stiffness**. In this study, and in consideration of the previous mentioned, it is proposed an **analysis of standardized pressures in a cell while it is being aspirated by a rectangular channel of a microfluidic device** through time using numerical CFD simulations and not considering viscoelastic effects that can make the mechanical behavior of the cell vary.

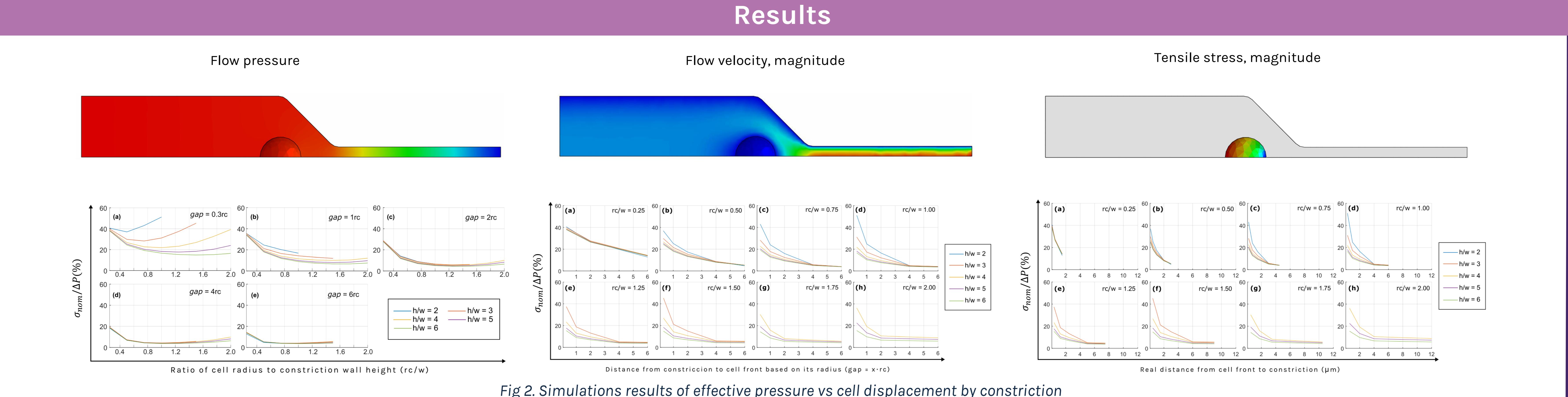
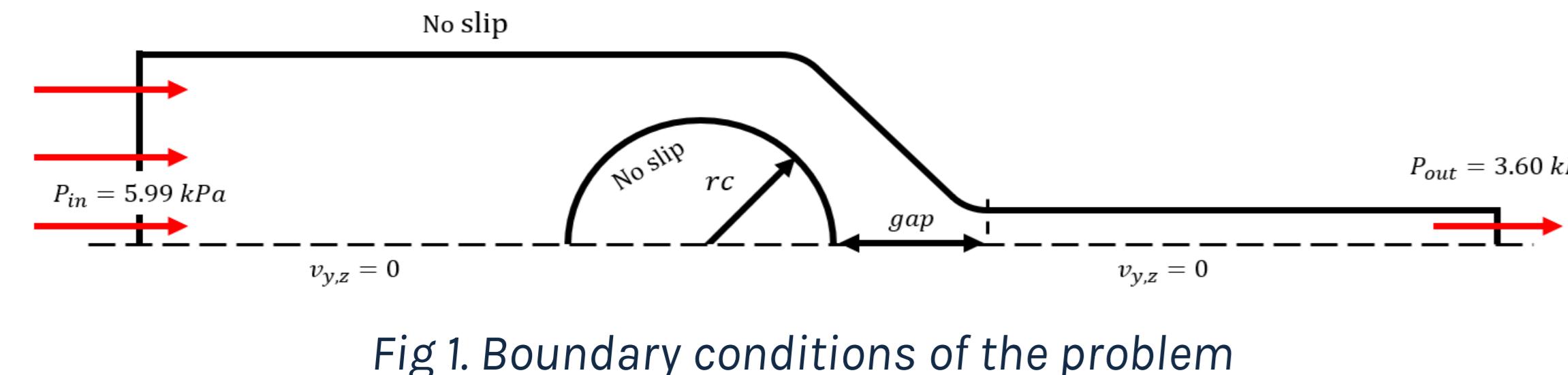
## Methods

The simulations focus on the pressure-velocity development of the fluid and leaving the structural analysis of the cell for a future work, so in each time step proposed, or distance traveled by the cell as it enters the duct, it is calculated independently from the previous one. When each simulation is finished, the tensions, in the direction of flow, on each surface element of the cell will be analysed and multiplied by its area to obtain the complete force on the simulated geometry quarter, which will be divided by its transversal area, being equal to the nominal tension  $\sigma_{nom} = F_{nom}/A$ . This nominal stress will finally be divided by the difference of pressures applied as a boundary condition, a quotient that **indicates how much the pressure of the flow on the cell surface is manifested**.

### Navier - Stokes Eq.

$$\rho \left( \frac{\partial \mathbf{v}}{\partial t} + \mathbf{v} \cdot \nabla \mathbf{v} \right) = -\nabla p + \mu \nabla^2 \mathbf{v} + \rho g$$

$$\mu \nabla^2 \mathbf{v} \gg \mathbf{v} \cdot \nabla \mathbf{v}$$

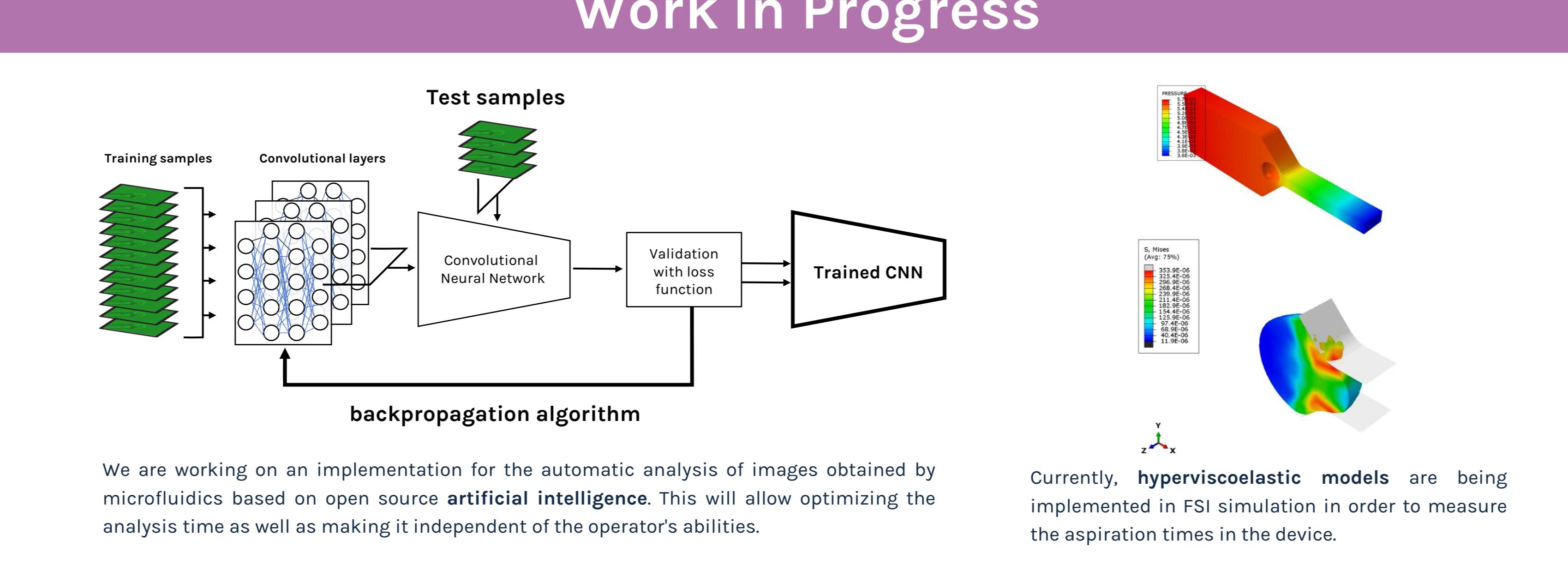


The analysis shows that the effective pressure increases inversely with the ratio of cell radius over width of the constriction, effect that is manifested when this is less than 1. **Just over half of the aspiration pressure is exerted on the cell effectively**, the rest of the pressure drop is mainly due to the movement of the fluid in the areas surrounding the cell in the rectangular cross section of the device, which will never be covered entirely by the cell as it happens in other techniques for measuring mechanical properties

## Conclusions

- The present work approaches the problem, of the **mechanical characterization of cells using a high performance microfluidic device**, utilizing numerical CFD simulations under different geometric configurations. Our model allows understanding the relationship between the deformation parameters and the deformability of the cell for a given aspiration pressure, which will be used in future analysis of deformability tests.
- The results indicate an increase in the effective pressure as it approaches the constriction. Pressure on the cell increases as the  $rc/w$  ratio is higher, that is, while it takes up more space in the duct. In all the cases studied, **the effective pressure is not much higher than 50%**.
- We need to obtain **new mathematical formulations** that consider the geometric configuration of both the device and the size of the cell under study.

## Work In Progress



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## References

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